

1 **Article**

2
3 **Title: Redox Nanoparticle Therapeutics to Cancer –Increase in therapeutic effect of**
4 **doxorubicin, suppressing its adverse effect–**

5
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26 **Competing Financial Interests statement**

27 No potential conflicts of interest were disclosed.

28

29

1 **ABSTRACT**

2 The ultimate goal of chemotherapy is to achieve a cure without causing any adverse effects.
3 We have developed pH-sensitive redox nanoparticle (RNP^N), which disintegrates under acidic
4 conditions and exposes nitroxide radicals, leading to strongly scavenging reactive oxygen species
5 (ROS). After intravenous administration of RNP^N to tumor bearing mice, it effectively
6 accumulated in tumor due to the leaky neovascular and immature lymphatic system and
7 scavenged ROS, resulting in suppression of inflammation and activation of NF- κ B, after
8 disintegration of RNP^N in tumor. Pre-administration of RNP^N prior to treatments with anticancer
9 agents, doxorubicin, to tumor-bearing mice significantly suppressed a progression of tumor size,
10 compared to low-molecular weight 4-hydroxy-TEMPO. Interestingly, the administration of
11 RNP^N suppressed adverse effects of doxorubicin to normal organs due to the scavenging ROS
12 and suppression of inflammation, which was confirmed by reduction in lactate dehydrogenase
13 and creatine phosphokinase activities in plasma. RNP^N is thus anticipated as novel and ideal
14 adjuvant for cancer chemotherapy.

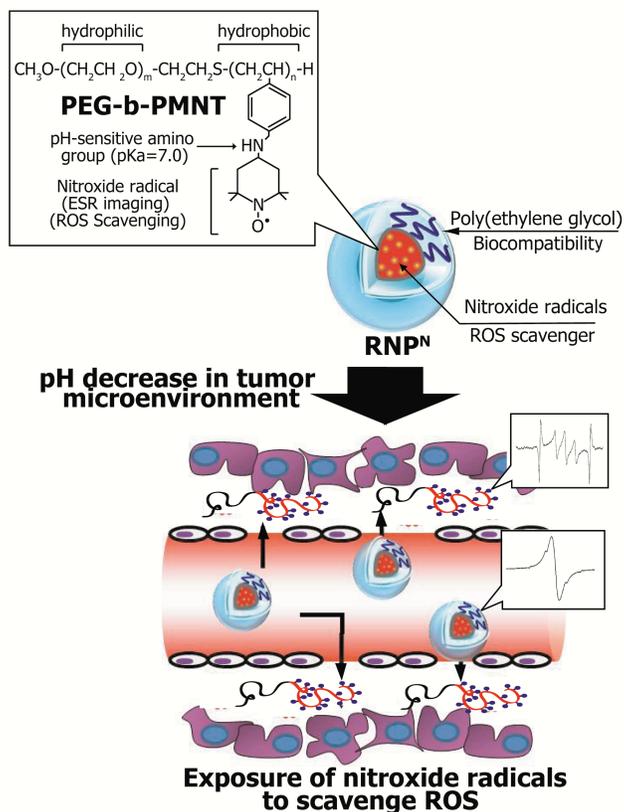
15 **Keywords:**

16 Nitroxide radical, pH-responsive polymeric micelle, reactive oxygen species, cancer
17 chemotherapy, doxorubicin, transcriptional factor

18 **Introduction**

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20
21 Despite years of anticancer drug development, including that of molecularly targeted
22 therapeutics with their ability to selectively interfere with certain hallmarks of cancer, no perfect
23 anticancer drug has been developed thus far. Cancer cells are known to develop drug resistance
24 with repeated drug administrations. Recently, chronic inflammation of the tumor
25 microenvironment has been reported to influence such drug resistance [1, 2]. Reactive oxygen
26 species (ROS) generated in this region play an important role [3]. Elevated rates of ROS have
27 been detected in almost all cancers [4], in which they activate transcription factors, such as
28 nuclear factor-kappa B (NF- κ B). It has been reported that this NF- κ B promotes many aspects of
29 tumor development and progression including an anti-apoptosis effect and drug resistance [5-7].
30 Interestingly, a large number of anticancer drugs such as the anthracyclines (e.g., doxorubicin
31 [DOX] epirubicin, and daunorubicin), alkylating agents, platinum coordination complexes (e.g.,
32 cisplatin, carboplatin, and oxaliplatin), epipodophyllotoxins (e.g., etoposide and teniposide), and
33 camptothecins (e.g., topotecan and irinotecan), generate ROS *in vivo*, resulting in severe adverse
34 effects in normal tissues [8, 9]. At the same time, these anticancer drugs increase oxidative
35 stress in tumor microenvironments and further increase drug resistance in this region. The
36 suppression of inflammation in the tumor microenvironment is one of the suitable targets for
37 decreasing drug resistance of tumor [9-13]. Several approaches have been reported thus far,
38 using anti-inflammatory agents and ROS scavengers such as dexamethasone (DEX) [10-12],
39 edaravone [13], and 2,2,6,6-tetramethylpiperidine-*N*-oxyl (TEMPO) [14]; pretreatment with
40 anti-inflammatory agents or ROS scavengers increases the antitumor activity of anticancer drugs.
41 However, *in vivo*, low-molecular-weight (LMW) drug-based approaches have limited potential
42 because they are rapidly excreted by the kidney [15], resulting in a lower concentration of drug
43 in the tumor area and severe adverse effects in normal tissue; for example, TEMPO derivatives
44 cause dramatic decrease in blood pressure after administration [16]. Additionally, a high
45 enough amount of LMW ROS scavengers cannot be used for the suppression of oxidative stress
46 in the tumor microenvironment, because LMW-TEMPO derivatives induce mitochondrial

1 dysfunction due to inessential redox reactions in the cells [17, 18].
2 To address these issues, we have focused on redox polymer therapeutics by using a nitroxide
3 radical-containing nanoparticle (RNP). We developed pH-sensitive RNP (RNP^N), which is a
4 core-shell type of self-assembling polymeric micelle that is 40 nm in diameter, prepared using
5 poly(ethylene glycol)-*b*-poly[4-(2,2,6,6-tetramethylpiperidine-*N*-oxyl)aminomethylstyrene]
6 (PEG-*b*-PMNT) diblock copolymer in aqueous media (Figure 1) [19-22]. As the leakage of the
7 drugs from the nanoparticle into the blood stream would decrease its therapeutic efficiency and
8 cause severe adverse effects, TEMPO moieties were covalently conjugated to the hydrophobic
9 segment of the amphiphilic block copolymer (PEG-*b*-PMNT). There are two main concepts
10 regarding RNP^N for delivering the nitroxide radical TEMPO to the tumor site and effectively
11 scavenging ROS. First, RNP^N exhibits long blood circulation time *in vivo* because of the
12 nanometer-sized structure and high biocompatibility of the PEG outer shell of RNP^N, resulting in
13 the accumulation of RNP^N in inflamed sites including the tumor area, because of the leaky
14 neovascular vessels in this area. Second, RNP^N disintegrates in response to acidic conditions
15 owing to the protonation of amino groups in the PMNT segments. Because of hypoxic effect in
16 tumor microenvironment, extracellular region of tumor is also acidic due to the increased
17 glycolytic system, referred to as Warburg effect [23]. Consequently, RNP^N must disintegrate not
18 only in endosome and lysosome but also in extracellular region of tumor, resulting in increased
19 ROS scavenging activity. Moreover, the adverse effect of LMW nitroxide radicals is markedly
20 suppressed as a result of the compartmentalization of nitroxide radicals in the core of RNP^N in
21 the bloodstream. Given these characteristics, it has so far been confirmed that RNP^N shows not
22 only a suppressive effect on oxidative stress in cellular studies [24, 25] but also a therapeutic
23 effect against ischemia reperfusion injury and intracerebral hemorrhage through intravenous
24 administration *in vivo* [26-28]. If RNP^N accumulates in tumor sites and scavenges ROS
25 effectively, drug resistance of tumor can be successfully prevented by the suppression of NF- κ B
26 activation. Another issue in the field of cancer chemotherapy is that the adverse effects of
27 anticancer drugs continue to trouble patients; for example, DOX causes severe cardiovascular
28 toxicity during chemotherapy. As stated previously, since RNP^N tends to improve blood
29 circulation, which increases accumulation in inflamed sites and effectively suppresses
30 inflammation by scavenging the generated ROS in these sites, adverse effects may decrease
31 because of the suppression of ROS caused by DOX in normal tissues. In this study, we
32 investigated the treatment effects of RNP^N on both the anti-tumor activity of DOX and
33 DOX-induced cardiotoxicity *in vivo*.
34



1
 2 **Figure 1.** Schematic illustration of (a) pH-sensitive RNP^N, which is a core-shell type of
 3 self-assembling polymeric micelle that is 40 nm in diameter and prepared using poly(ethylene
 4 glycol)-*b*-poly[4-(2,2,6,6-tetramethylpiperidine-*N*-oxyl)aminomethylstyrene] (PEG-*b*-PMNT)
 5 amphiphilic diblock copolymers; and (b) the effective accumulation and disintegration of RNP^N
 6 in the tumor area

7
8
9 **Material and Methods**

10 **Preparation of RNP^N**

11 pH-responsive RNP^N was prepared using self-assembling PEG-*b*-PMNT block copolymers, as
 12 previously reported [20]. Please see Supplementary Methods about detailed description of the
 13 method.

14
15 **Animal**

16 The experiments on the enhancement of anticancer activity and cardiotoxicity of DOX
 17 were carried out using BALB/c (4 weeks old, male, approximately 25 g) and ICR mice (7 weeks
 18 old, male, approximately 35 g), respectively, that were purchased from CHARLES RIVER
 19 JAPAN, Inc. Mice were maintained in the experimental animal facilities at the University of
 20 Tsukuba. All mice were housed in a temperature- and humidity-controlled, 12-h light:12-h
 21 dark environment. All mice were fed commercial chow and water ad libitum. All
 22 experiments were performed according to the Guide for the Care and Use of Laboratory Animals
 23 of the University of Tsukuba.

1 **Electron spin resonance (ESR) measurement of nitroxide radical concentration in blood**
2 **and tumors.**

3 The biodistribution of the nitroxide radicals in the RNP^N in tumor-bearing mice was
4 evaluated using ESR. The tumor-bearing mice were prepared with a subcutaneous injection of
5 murine colon adenocarcinoma 26 (colon-26) cells (1×10^6 cells/mouse) into their right thigh.
6 When the volume of the tumor reached 100 mm³, RNP^N (300 mg/kg) or 4-hydroxy-TEMPO
7 (TEMPOL) (40 mg/kg) was administered to the tumor-bearing mice by intravenous injection.
8 It should be noted that the concentrations of nitroxide radicals in all drugs were the same, which
9 were adjusted using ESR measurements. Blood samples were collected from the heart using a
10 heparinized syringe at 0.083, 0.25, 1, 3, 6 and 24 h after administration, and the tumor was
11 excised immediately after blood collection. The blood and tumor were immediately placed on
12 ice. Plasma samples were then obtained by centrifuging (6,200 rpm, 2000 g, for 10 min) the
13 blood samples. To determine the ESR intensities at 0 min, 12.5 μL of RNP^N solution (30
14 mg/mL) was added to the blood (100 μL), followed by centrifugation (6,200 rpm, 2000 g, for 10
15 min) of the blood and the measurement of ESR, assuming that the total blood volume in mice is
16 80 mL/kg. The tumor tissue homogenates were prepared using an ultra-sonic homogenizer
17 (UH-50; SMT Company, Tokyo, Japan).

18 Nitroxide radicals are reduced to hydroxylamine, which has no ESR signal, by an *in vivo*
19 reducing agent such as ascorbic acid. As hydroxylamine also possesses ROS-scavenging
20 capacity, the total drug concentrations (nitroxide radicals + hydroxylamines) in blood and tumor
21 were determined by the addition of potassium ferricyanide (K₃[Fe(CN)₆]) (200 mM, 20 μL) to
22 plasma (200 μL) or the tumor homogenate sample (200 mg) to re-oxidize the hydroxylamines to
23 nitroxide radicals. Using an X-band ESR spectrometer (JES-TE25X; JEOL, Tokyo, Japan), the
24 ESR measurements were carried out under the following conditions: frequency, 9.41 GHz;
25 power, 8.00 mW; field, 333.8 ± 5 mT; sweep time, 1.0 min; modulation, 0.1 mT; and time
26 constant, 0.1 s.

27
28 ***In vivo* antitumor activity studies**

29 Tumor-bearing mice were randomly divided into various treatment and control groups (5
30 mice/group). Animals were treated with saline, RNP^N (100 mg/kg) or LMW-TEMPOL (13.3
31 mg/kg) by intravenous injection once per day for 4 days before chemotherapy (days -4 to -1).
32 DOX was administered intravenously at a single dose of 10 mg/kg on day 0. Antitumor activity
33 was evaluated in terms of tumor volume (V), which was calculated using the following equation:

$$34 \text{ Tumor volume (V)} = 0.52 \times L \times W^2$$

35 L and W are the long diameter and the short diameter of the tumor, respectively, as measured by
36 a caliper.

37
38 **Western blot analysis.**

39 The protein levels of nuclear NF-κB (p65) were measured by Western blotting. The
40 colon 26 cell was used for the *in vitro* study, similar to the *in vivo* study using tumor-bearing
41 mice. The protein from control and RNP^N-treated cells was extracted using a nuclear extraction
42 kit (Cayman Chemical Company, Ann Arbor, MI, USA) according the manufacturer's protocol.
43 Protein estimation was carried out using the Thermo Scientific Pierce BCA Protein Assay Kit
44 (Rockford, IL, USA). Approximately 20 μL of protein sample was electrophoresed in a 15%
45 polyacrylamide gel and transferred to a nitrocellulose membrane (Bio-Rad, Richmond, CA,
46 USA) by electroblotting. The membrane was blocked for 1 h with 1% BSA and probed with

1 the primary and secondary antibodies. Luminata™ Western HRP Substrate (EMD Millipore
2 Corporation, Billerica, MA, USA) was used to develop the membrane and the protein
3 concentrations were estimated. Each blot was stripped and reprobed for β -actin for equal
4 protein loading detection.

6 **Evaluation of the suppressive effect of RNP^N on cardiotoxicity caused by DOX**

7 The ICR mice were randomly divided to receive an intravenous injection of DOX (20
8 mg/kg) 30 min after the intravenous injection of RNP^N (25 mg/kg), LMW-TEMPOL (4 mg/kg),
9 or phosphate-buffered saline (PBS), followed by 2 intravenous injections of RNP^N (25 mg/kg),
10 LMW-TEMPOL (4 mg/kg), or PBS at 24 and 48 h after DOX administration. At 72 h after
11 DOX administration, the mice were anesthetized and blood samples were collected by
12 intracardiac puncture using a heparinized syringe. Plasma samples were then obtained by
13 centrifugation (6,200 rpm, 2000 g, for 10 min) of the blood. Plasma samples were assayed for
14 plasma lactate dehydrogenase (LDH) and plasma creatine phosphokinase (CPK) activities using
15 a Fuji Dri-chem 3500 analyzer (Fuji-Film, Tokyo, Japan). To determine the amounts of lipid
16 peroxidation and superoxide induced by DOX, heart tissues were excised from mice after the
17 blood samples were collected. Plasma and heart tissue were frozen and stored at -80 °C until
18 the further use.

20 **Measurement of levels of superoxide anion, TNF- α , and malonyldialdehyde (MDA)**

21 Please see Supplementary Methods about detailed description of the method.

23 **Statistical analysis**

24 All values are expressed as mean \pm standard error of mean (SEM). Differences
25 between two groups were examined for statistical significance by using the Student's *t* test.
26 Differences between more than three groups were examined for statistical significance by using
27 one-way ANOVA followed by Tukey's test (SPSS software; IBM Corp, Armonk, NY, USA). A
28 P value of <0.05 was considered significant for all of these statistical analyses.

30 **Results**

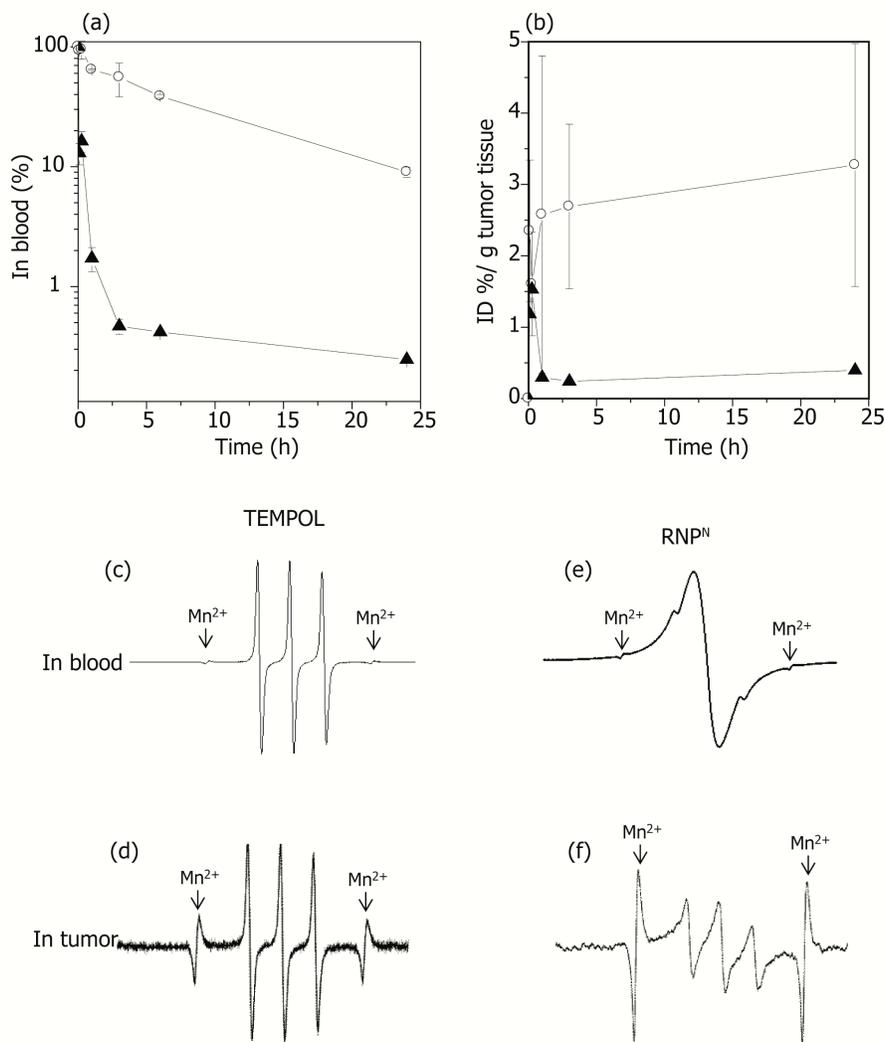
31 **Biodistribution of RNP^N and its morphological change in tumor sites**

32 PEG-*b*-PMNT block copolymers were prepared as previously reported [20]. RNP^N was prepared
33 by self-assembly of the synthesized amphiphilic block copolymer, PEG-*b*-PMNT, via the
34 dialysis method against water, with an average diameter of about 40 nm (polydispersity factor,
35 $\mu/\Gamma^2 = 0.04$). To examine the biodistribution of RNP^N and LMW-TEMPOL in tumor-bearing
36 mice, we measured the concentration of nitroxide radicals in the blood and tumor area by ESR,
37 because nitroxide radicals are susceptible to ESR. Figure 2a shows the time profile of the drug
38 concentration of RNP^N and LMW-TEMPOL in the blood. Contrary to the rapid clearance of
39 LMW LMW-TEMPOL from the bloodstream, the ESR signals of RNP^N were observed for a
40 relatively long period of time. The AUC value of RNP^N in blood (AUC: 769.49) was much
41 higher than that of LMW-TEMPOL (AUC: 19.2). The rapid clearance of LMW-TEMPOL
42 might be attributed to preferential renal clearance and diffusion across the entire body. Figure
43 2b shows the accumulation amounts of RNP^N and LMW-TEMPOL in tumors. The
44 accumulation level of RNP^N in the tumor tissues of mice at 24 h after intravenous administration
45 was 3.3% ID/g tumor tissue, whereas that of LMW-TEMPOL at 24 h after injection was only
46 0.4% ID/g tumor tissue. Although the accumulation tendency of RNP^N was not markedly higher

1 than that of RNP^O, another nitroxide radical-containing nanoparticles that is not pH-sensitive and
2 has high colloidal dispersion stability (see Figures S1 and S2), the AUC of RNP^N in tumor
3 tissues (AUC: 39.6) was still 6 to 7 fold higher than that of LMW-TEMPOL (AUC: 6.5). This
4 indicated the clear accumulation of nanoparticles in tumors because of the increased vascular
5 permeation and immature lymphatic excretion (the so-called enhanced permeability and retention
6 [EPR] effect [29]). The moderate accumulation tendency of RNP^N is probably due to the
7 pH-disintegration characteristics (see below) of the polyamine segment, which may loosen its
8 coagulation force coagulation force of hydrophobic interaction in the core by increasing its
9 hydrophilicity. The validity of our strategy regarding the covalent conjugation of bioactive
10 species, nitroxide radicals, in this case, was demonstrated. If the physical entrapment of
11 TEMPO molecules in pH-sensitive nanoparticles is used, they must leak easily during circulation
12 due to the loosened core.

13 The ESR spectra of RNP^N can provide information on morphological changes *in vivo*.
14 The ESR signal of LMW-TEMPOL derivatives shows a sharp triplet due to an interaction between
15 the 14-nitrogen nuclei and the unpaired electron in the dilute solution. At 15 min after the
16 intravenous administration of LMW-TEMPOL to mice, clear triplet signals were observed both
17 in blood and in tumors, as shown in Figures 2c and 2d. In contrast, the ESR signal of RNP^N in
18 the blood stream showed a broad spectrum, because of the confinement of the nitroxide radicals
19 in the solid core of RNP^N (Figure 2e). As shown in Figure 2f, the triplet signals were observed
20 in tumor, indicating the disintegration of RNP^N in this area and the exposed nitroxide radicals
21 outside of the particle, which is probably due to the acidic tumor microenvironment. In fact, no
22 changes in ESR signals for both blood and tumor were observed for RNP^O (Figure S3), leading
23 us to strongly anticipate an increase in the reactivity of the nitroxide radicals of RNP^N to ROS in
24 tumors as a result of its disintegration at the tumor sites.

25

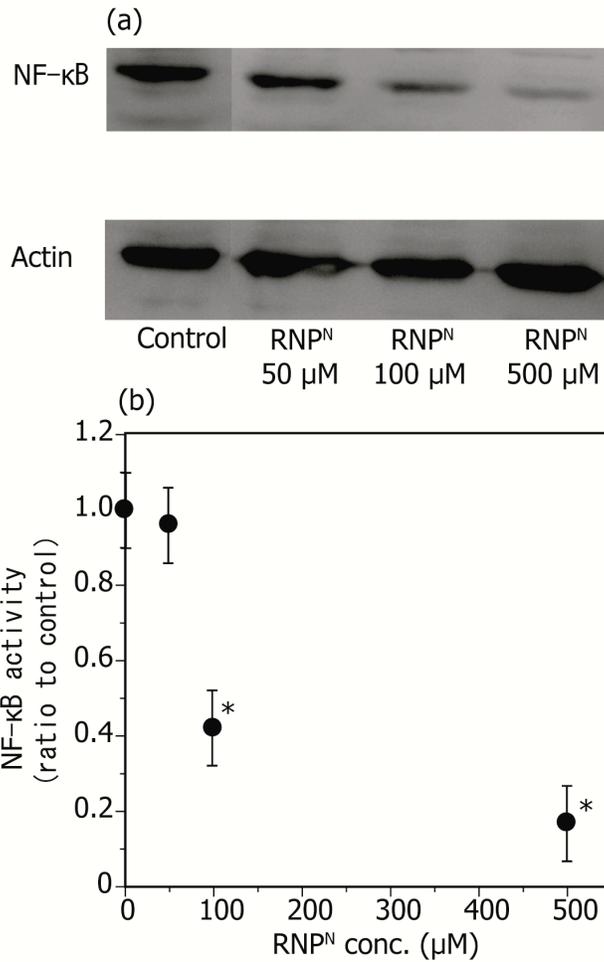


1
 2 **Figure 2.** (a,b) Distribution profiles of RNP^N (white circle) and low-molecular-weight (LMW)
 3 4-hydroxy-2,2,6,6-tetramethylpiperidine-*N*-oxyl (TEMPOL) (block triangle) in (a) blood and (b)
 4 tumor tissue from tumor-bearing mice, as determined by electron spin resonance (ESR)
 5 measurement. The data are expressed as means \pm SEM; $n = 5$. (c-f) The ESR spectra of (c)
 6 LMW-TEMPOL in blood, (d) LMW-TEMPOL in tumor, (e) RNP^N in blood, and (f) RNP^N in
 7 tumor at 15 min after intravenous administration are shown. All samples were oxidized by
 8 potassium ferricyanide ($K_3[Fe(CN)_6]$).

9
 10
 11 **Pretreatment of tumor-bearing mice with RNP^N enhances the therapeutic effects of DOX *in***
 12 ***vivo***

13 Having confirmed that RNP^N accumulates and disintegrates in tumor regions, we
 14 investigated the effect of RNP^N on the expression of NF- κ B in cancer cells. Figure 3 shows the
 15 expression level of NF- κ B in the nuclei of colon-26 cells with and without RNP^N treatment. In
 16 contrast to the high expression level of NF- κ B observed in the nuclei of tumor cells, the
 17 expression level of NF- κ B was suppressed, in a dose-dependent manner, on administration of
 18 RNP^N, clearly indicating the effectiveness of RNP^N in suppressing this transcription factor in

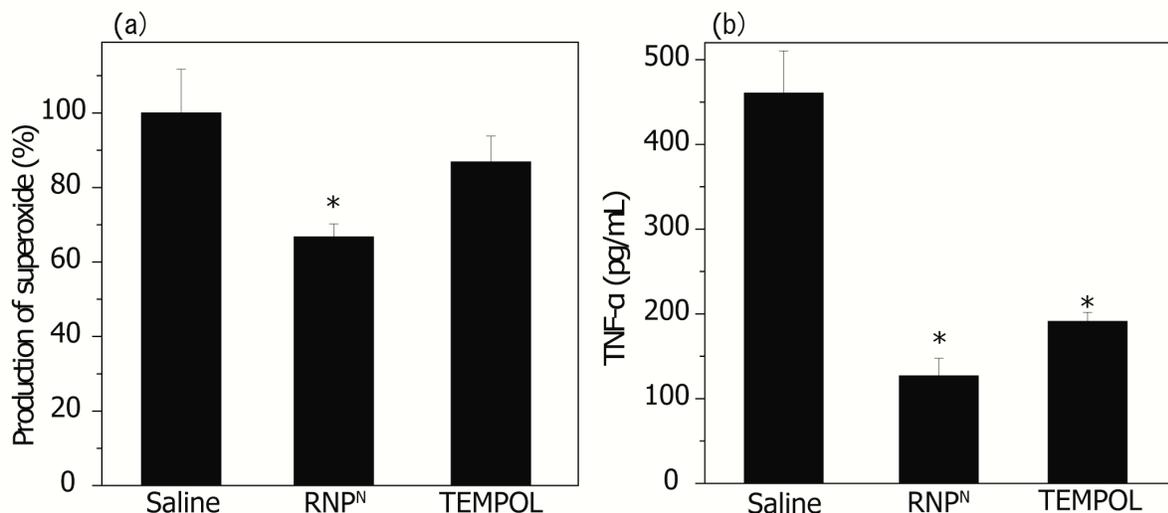
1 colon-26 cells.
2



3
4 **Figure 3.** Suppressive effects of RNP^N on the activation of NF-κB. (a) Western blot analysis
5 of NF-κB expression in colon-26 cells treated with RNP^N. (b) The graph represents the
6 densitometry average of three representative blots. Values are expressed as mean ± SEM. **P*
7 < 0.05 compared with controls; Student's *t*-test; n = 3.

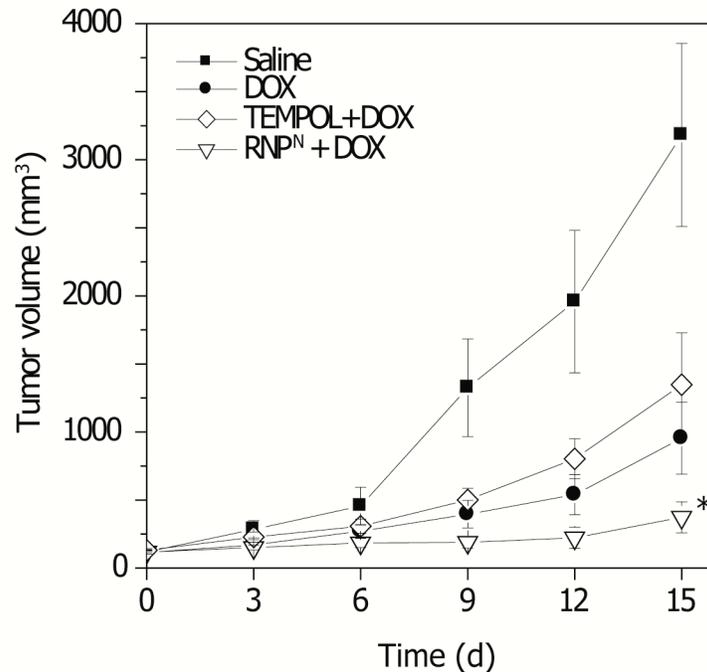
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9 Given the significant effect of RNP^N observed on the suppression of inflammatory
10 transcription factor NF-κB, we investigated the pharmacological effect of the anticancer drug,
11 DOX, after pretreatment of tumor-bearing mice with RNP^N. Here, RNP^N was administered for 4
12 days to suppress the NF-κB activation before DOX treatment. First, we measured the suppressive
13 effect of RNP^N treatment on superoxide generation in the tumor area. Because PEG-b-PMNT
14 possesses nitroxide radicals, it scavenges ROS such as superoxide and hydroxyl radicals [30].
15 When tumor-bearing mice were treated with intravenous injections of RNP^N at a dose of 100
16 mg/kg for 4 days, the levels of ROS were found to be significantly decreased in tumors
17 compared with controls (saline administration); this is in sharp contrast to the results observed
18 with administration of LMW-TEMPOL (Figure 4a). The suppression of oxidative stress in the
19 tumor microenvironment was also confirmed by the measurement of the proinflammatory
20 cytokine, TNF-α. As seen in Figure 4b, the suppressive effect of RNP^N treatment on level of

1 TNF- α was higher than that of LMW-TEMPOL. These findings underline the importance of
2 local ROS scavenging by RNP^N, which results in the suppression of cytokine levels and NF- κ B
3 activation [31], resulting in the inhibition of tumor resistance.
4



5
6 **Figure 4.** Suppressive effect of pretreatment with RNP^N on the generation of superoxide
7 anions and TNF- α in tumors. (a) Amounts of superoxide in tumor tissue were measured using
8 dihydroethidium (DHE). Superoxide values were expressed as the value related to the
9 fluorescent intensity of the saline group. Values are expressed as mean \pm SEM. * P < 0.05
10 compared with the saline group; ANOVA; n = 5. (b) The concentration of TNF- α in tumor was
11 measured by enzyme-linked immunosorbent assay (ELISA). Values are expressed as mean \pm
12 SEM. * P < 0.05 compared with the saline group; ANOVA; n = 10.
13

14 Having demonstrated the suppression of inflammation in the tumor microenvironment
15 and the activation of inflammatory transcription factor NF- κ B, we then examined the enhancing
16 effect of RNP^N on the anti-tumor activity of DOX. Tumor-bearing mice were treated with
17 intravenous injections of RNP^N at a dose of 100 mg/kg for 4 days (days -4 to -1), followed by the
18 intravenous injection of DOX (10 mg/kg, day 0). Tumor progression was analyzed as shown in
19 Figure 5. When LMW-TEMPOL was administered intravenously and followed by DOX
20 administration, almost no effect was observed. Although it was previously reported that the
21 intratumoral administration of TEMPO in tumor-bearing mice inhibits tumor growth by inducing
22 apoptosis [14], the intravenous administration of LMW-TEMPOL in tumor-bearing mice did not
23 show any effect under the present study conditions. The reason for these results may stem from
24 a lower intratumoral concentration of nitroxide radicals because of rapid renal clearance and
25 diffusion throughout the entire body. In contrast, a remarkably large effect was observed with
26 the administration of RNP^N prior to DOX administration. Interestingly, a much higher adjuvant
27 effect of RNP^N on the anti-tumor activity of DOX was observed *in vivo* compared with that of
28 RNP^O, although the tumor accumulation of RNP^O was much higher than that of RNP^N (Figure
29 S4). This result indicates that both accumulation tendency and pH-triggered disintegration
30 characteristics of RNP^N are important to effectively suppress the activation of NF- κ B and
31 decrease the resistance of tumor cells. Similar effects were observed with the pretreatment of
32 RNP^N prior to the administration of other anticancer drugs, carboplatin (Figure S5).
33

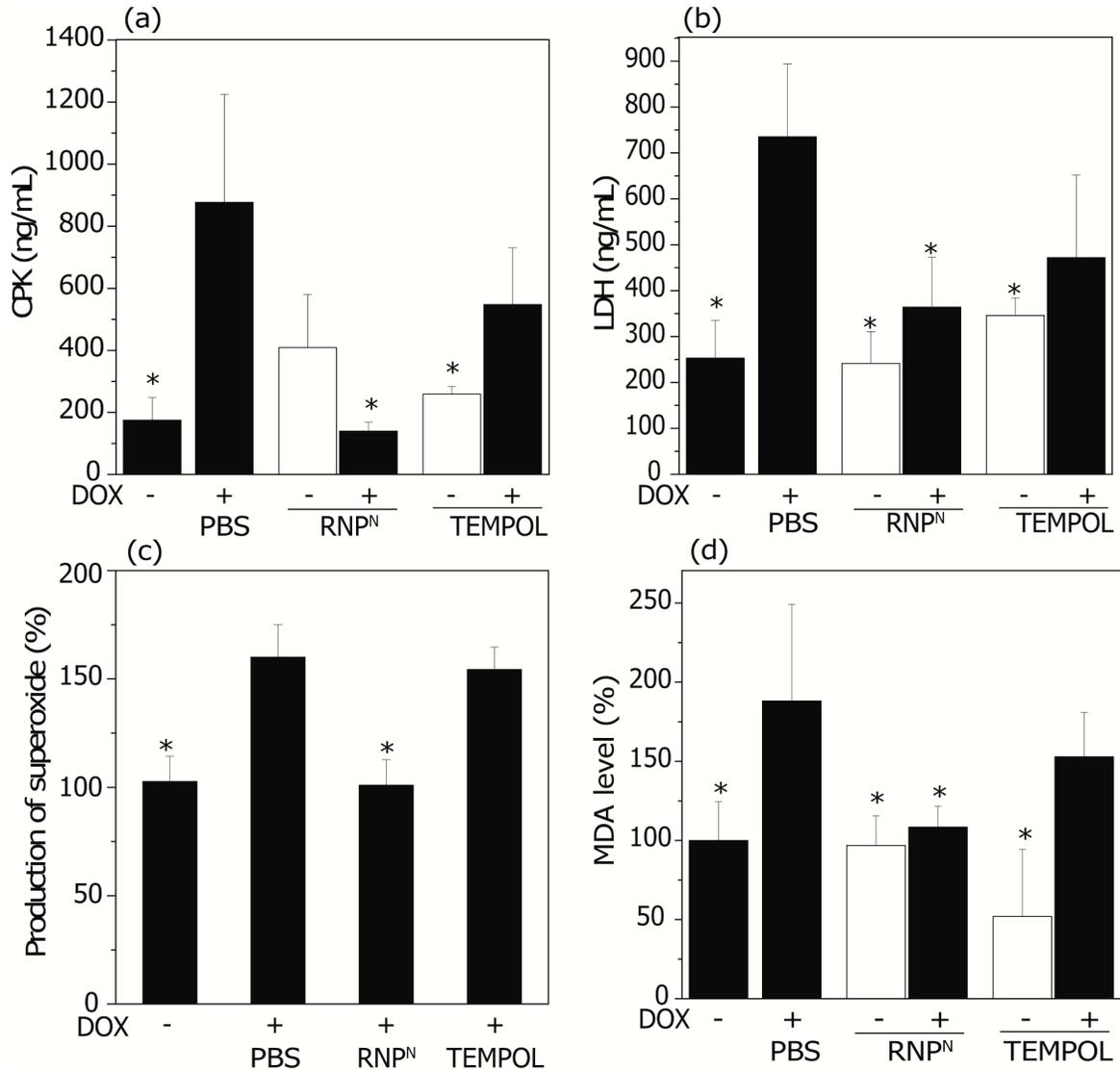


1 **Figure 5.** Effect of RNP^N pretreatment on the antitumor activity of doxorubicin (DOX) in
 2 BALB/c mice bearing colon-26 tumors. Animals were intravenously pretreated with RNP^N
 3 (100 mg/day for 4 days, days -4 to -1). DOX was intravenously administered at a single dose of
 4 10 mg/kg on day 0. Tumor size is expressed as mean \pm SEM. * $P < 0.05$ compared with DOX
 5 alone; Student's t -test; $n = 5$.
 6

9 **Suppression of adverse effects of DOX by RNP^N**

10 DOX is known to cause cardiotoxicity through the generation of ROS as stated previously.
 11 We have already confirmed that RNPs tend to accumulate in inflammation sites and effectively
 12 suppress inflammation by scavenging ROS generated in these sites [32]. If RNP^N suppresses
 13 the adverse cardiotoxic effects of DOX in addition to inhibiting tumor progression, it would be
 14 an ideal cancer chemotherapy system. To examine the cardiotoxicity of DOX, CPK and LDH
 15 activities were measured. CPK, LDH, which are indicator of myocardial damage, are released
 16 from the heart muscle cells when it is injured. Here, RNP^N or LMW-TEMPOL was administered
 17 three times before and after DOX treatment because DOX generates ROS continuously not only
 18 in tumor region but also in healthy organs such as heart and liver. As shown in Figures 6a and
 19 6b, compared to that of mice given a tail vein injection of PBS, mice treated with a single dose of
 20 DOX (20 mg/kg) showed a 5-fold increase in plasma CPK activity and a 2.9-fold increase in
 21 plasma LDH activity. Although the administration of LMW-TEMPOL showed decreases in
 22 plasma CPK and LDH activities to some extent in DOX-treated mice, no significant difference
 23 was found. In contrast, the administration of RNP^N (100 mg/kg) for 3 days remarkably
 24 suppressed cardiotoxicity in DOX-treated mice, as determined by reduction in CPK and LDH.
 25 We also investigated whether pretreatment with RNP^N could scavenge ROS, particularly
 26 superoxide, generated in the heart at 24 h after DOX administration. As shown in Figure 6c,
 27 the generation of ROS in heart tissue was significantly inhibited by RNP^N treatment, regardless
 28 of the lack of effect observed with LMW-TEMPOL treatment. Cardiotoxicity was also

1 investigated by determining the level of lipid peroxidation in the heart after DOX administration.
 2 When 20 mg/kg of DOX was administered intravenously, the level of MDA in the heart
 3 increased significantly (Figure 6d). In contrast, no increase was observed with a 3-day
 4 RNP^N-treatment before and after DOX administration; again, this is in sharp contrast to the
 5 findings obtained with LMW-TEMPOL. These results can be attributed to the long circulation
 6 time of RNP^N in blood and the accumulation of RNP^N in the inflamed area, followed by the
 7 effective scavenging of ROS, resulting in the suppression of cardiotoxicity caused by DOX.
 8



9
 10 **Figure 6.** (a,b) Effect of treatment with RNP^N or
 11 4-hydroxy-2,2,6,6-tetramethylpiperidine-*N*-oxyl (TEMPOL) on doxorubicin (DOX)-induced
 12 cardiotoxicity, as determined by measurement of the activities of (a) creatine phosphokinase
 13 (CPK) and (b) lactate dehydrogenase (LDH) in plasma. The bar graphs represent means ± SEM,
 14 **P* < 0.05 compared with DOX alone; Student's *t*-test; *n* = 6. (c) Amounts of superoxide in heart
 15 tissue were measured using dihydroethidium (DHE). Superoxide values were expressed as the
 16 value related to the fluorescent intensity of the control group. Values are expressed as mean ±
 17 SEM. **P* < 0.05 compared with DOX alone; ANOVA; *n* = 4. (d) Effect of treatment with

1 RNP^N or LMW-TEMPOL on malonyldialdehyde (MDA) activity in the heart tissue of ICR mice
2 after DOX administration. Values are expressed as mean ± SEM. **P* < 0.05 compared with
3 DOX alone; Student's *t*-test; n = 6.

6 Discussion

7 ROS are involved in the development of a wide spectrum of diseases, including chronic
8 inflammation and cancers. Anticancer drugs administered to cancer patients induce excessive
9 oxidative stress, leading to further inflammation and ROS production. This negative cycle
10 induces the expression of transcription factors such as NF-κB and initiates many factors such as
11 anti-apoptotic effects and drug resistance, leading to tumor development and progression; these
12 factors lower the therapeutic effects of the anticancer drug and cause serious adverse effects. A
13 combination therapy of anticancer drugs with anti-inflammatory agents or ROS scavengers has
14 been developed and applied in treatment. However, this therapy has not been very effective
15 because of the rapid elimination of LMW drugs from the body via renal clearance [15] and the
16 severe adverse effects of the drugs in normal tissues [16-18].

17 In this study, we demonstrated that RNP^N suppresses the activation of transcription factor,
18 NF-κB in the cancer cells and improves the anticancer effect of DOX in vivo. These results
19 indicate that long-term and effective ROS scavenging at the tumor site by RNP^N pretreatment
20 enhances the anticancer effect of the drug, because of effective accumulation and disintegration
21 of RNP^N in the tumor area. Inflammatory cytokines are also suppressed by RNP^N treatment.
22 Production of ROS and inflammatory cytokines has been proven to be strongly associated with
23 each other [33]. We have observed that ROS scavenging suppresses the production of
24 inflammatory cytokines. RNP^N showed an extended period of circulation in the blood and
25 accumulation in inflamed areas, and the cardiac toxicity of DOX was reduced by RNP^N treatment.
26 Moreover, the anticancer activity and suppression of adverse effects was more remarkably
27 enhanced by RNP^N than by LMW-TEMPOL. Since almost all the anticancer drugs have some
28 drawbacks such as low efficiency and adverse effects, we believe that RNP^N system can help
29 design improved cancer treatments with good therapeutic outcomes, suppressing the adverse
30 effects of the drugs.

32 Conclusions

33 In conclusion, we have demonstrated that the pretreatment of our newly designed
34 pH-responsive redox nanoparticle (RNP^N), which tends to accumulate and disintegrate in tumor
35 area, enhances the anti-tumor activity of DOX, because the exposed nitroxide radicals effectively
36 scavenge ROS, which suppress the activation of NF-κB in this area. Our findings also showed
37 that RNP^N protects the cardiac damage by DOX in vivo. It should be noted that LMW-TEMPOL
38 did not show these effects, which was probably due to its non-specific dispersion in entire body.
39 This approach is based on the redox-nanoparticle assisted suppression of oxidative stress in
40 tumor microenvironment, which may open a new paradigm for the design of improved cancer
41 treatments with high chemotherapeutic outcomes, suppressing their adverse effects.

43 Acknowledgments

44 We would like to thank Nobuko Nishizawa and Umeko Horiuchi (Graduate School of Pure and
45 Applied Sciences, University of Tsukuba) for their technical assistance. Part of this work was
46 supported by a Grant-in-Aid for Scientific Research A (21240050) and the World Premier

1 International Research Center Initiative (WPI Initiative) on Materials Nanoarchitronics from the
2 Ministry of Education, Culture, Sports, Science and Technology (MEXT) of Japan.

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34

1 **Figure Legends:**

2
3 **Figure 1.** Schematic illustration of (a) pH-sensitive RNP^N, which is a core-shell type of
4 self-assembling polymeric micelle that is 40 nm in diameter and prepared using poly(ethylene
5 glycol)-*b*-poly[4-(2,2,6,6-tetramethylpiperidine-*N*-oxyl)aminomethylstyrene] (PEG-*b*-PMNT)
6 amphiphilic diblock copolymers; and (b) the effective accumulation and disintegration of RNP^N
7 in the tumor area.

8
9 **Figure 2.** (a,b) Distribution profiles of RNP^N (white circle) and low-molecular-weight (LMW)
10 4-hydroxy-2,2,6,6-tetramethylpiperidine-*N*-oxyl (TEMPOL) (block triangle) in (a) blood and (b)
11 tumor tissue from tumor-bearing mice, as determined by electron spin resonance (ESR)
12 measurement. The data are expressed as means \pm SEM; n = 5. (c-f) The ESR spectra of (c)
13 LMW-TEMPOL in blood, (d) LMW-TEMPOL in tumor, (e) RNP^N in blood, and (f) RNP^N in
14 tumor at 15 min after intravenous administration are shown. All samples were oxidized by
15 potassium ferricyanide (K₃[Fe(CN)₆]).

16
17 **Figure 3.** Suppressive effects of RNP^N on the activation of NF- κ B. (a) Western blot analysis
18 of NF- κ B expression in colon-26 cells treated with RNP^N. (b) The graph represents the
19 densitometry average of three representative blots. Values are expressed as mean \pm SEM. **P*
20 < 0.05 compared with controls; Student's *t*-test; n = 3.

21
22 **Figure 4.** Suppressive effect of pretreatment with RNP^N on the generation of superoxide
23 anions and TNF- α in tumors. (a) Amounts of superoxide in tumor tissue were measured using
24 dihydroethidium (DHE). Superoxide values were expressed as the value related to the
25 fluorescent intensity of the saline group. Values are expressed as mean \pm SEM. **P* < 0.05
26 compared with the saline group; ANOVA; n = 5. (b) The concentration of TNF- α in tumor was
27 measured by enzyme-linked immunosorbent assay (ELISA). Values are expressed as mean \pm
28 SEM. **P* < 0.05 compared with the saline group; ANOVA; n = 10.

29
30 **Figure 5.** Effect of RNP^N pretreatment on the antitumor activity of doxorubicin (DOX) in
31 BALB/c mice bearing colon-26 tumors. Animals were intravenously pretreated with RNP^N
32 (100 mg/day for 4 days, days -4 to -1). DOX was intravenously administered at a single dose of
33 10 mg/kg on day 0. Tumor size is expressed as mean \pm SEM. **P* < 0.05 compared with DOX
34 alone; Student's *t*-test; n = 5.

35
36 **Figure 6.** (a,b) Effect of treatment with RNP^N or
37 4-hydroxy-2,2,6,6-tetramethylpiperidine-*N*-oxyl (TEMPOL) on doxorubicin (DOX)-induced
38 cardiotoxicity, as determined by measurement of the activities of (a) creatine phosphokinase
39 (CPK) and (b) lactate dehydrogenase (LDH) in plasma. The bar graphs represent means \pm SEM,
40 **P* < 0.05 compared with DOX alone; Student's *t*-test; n = 6. (c) Amounts of superoxide in heart
41 tissue were measured using dihydroethidium (DHE). Superoxide values were expressed as the
42 value related to the fluorescent intensity of the control group. Values are expressed as mean \pm
43 SEM. **P* < 0.05 compared with DOX alone; ANOVA; n = 4. (d) Effect of treatment with
44 RNP^N or LMW-TEMPOL on malonyldialdehyde (MDA) activity in the heart tissue of ICR mice
45 after DOX administration. Values are expressed as mean \pm SEM. **P* < 0.05 compared with
46 DOX alone; Student's *t*-test; n = 6.